

Quantum Dots' Role in Cancer Diagnosis: An overview on Nano-Fluorescence in Oncology

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Abstract

This paper highlights the significant advantages of utilizing quantum dots (QDs) in cancer detection. The discussion begins with an introduction to Quantum Dots and Their Properties, emphasizing their unique characteristics. Subsequently, the paper explores the utility of Quantum Dots as Imaging Probes, shedding light on their role in enhancing imaging capabilities for cancer diagnosis. The focus then shifts to their pivotal role in cancer targeting, particularly for early detection. Finally, Challenges and Future Prospects in the field of QD-based cancer detection are addressed. This comprehensive overview underscores the potential of quantum dots in revolutionizing cancer diagnosis and opens avenues for further research and development.

Keywords: Nanotechnology; Nanomedicine; Quantum Dots; Cancer Detection; Imaging Probes; Early Detection

Abbreviations: CT: Computed Tomography; PET: Positron Emission Tomography; MRI: Magnetic Resonance Imaging; FRET: Förster Resonance Energy Transfer; RES: Reticuloendothelial System.

Introduction

Quantum dots (QDs) represent a class of nanomaterials renowned for their distinctive chemical and physical characteristics. Their capacity to confine charges, such as electrons and holes, within three dimensions grants us precise control over their energy levels and wave functions, ultimately bestowing upon them remarkable luminescent and absorptive properties. These unique properties have made them a vital nanostructure for a wide variety of applications in various fields such as optoelectronics, biomedical imaging, solar cells, quantum computing, and advanced materials science [1-6]. Hence, in the year 2023, three pioneers in the field of nanotechnology—namely, Bawendi, Louis E. Brus, and Alexei I. Ekimov—were honored with a Nobel Prize for their groundbreaking contributions. These laureates are celebrated for their pivotal roles in the discovery and development of QDs, semiconductors compressed to such minuscule scales that their electrons find themselves in exceptionally confined carriers, which has unlocked a realm of unprecedented possibilities [7-10].

Cancer diagnosis hinges on a range of sophisticated imaging techniques, each with its unique advantages and applications [11]. These modalities encompass ultrasound, X-rays, computed tomography (CT) [12], positron emission tomography (PET) [13], magnetic resonance imaging (MRI) [14], and more. Ultrasound, for example, employs highfrequency sound waves to create real-time images and is often employed for the assessment of solid tumors and blood flow evaluation across various cancer types. X-rays are invaluable

for detecting abnormalities, particularly in breast and lung cancer screenings. Computed tomography (CT) merges X-ray technology with computer processing to produce detailed cross-sectional images, making it essential for visualizing tumor size and location. Positron emission tomography (PET) offers valuable insights into metabolic activity within tissues, helping identify areas of concern. Magnetic resonance imaging (MRI) harnesses strong magnets and radio waves to produce detailed anatomical images, proving particularly useful in visualizing soft tissues and detecting cancer in organs like the brain, breast, and prostate. These diagnostic tools, in conjunction with emerging technologies, serve as critical assets for early cancer detection and precise characterization, ultimately enhancing treatment strategies and elevating patient outcomes. Targeted treatment's effectiveness depends on the presence of the specific genetic change or protein that the drug targets within the tumor [15-17]. However, even when the target is present, the tumor's response to the drug may vary, and the treatment's durability over time can be unpredictable.

In recent years, the distinctive characteristics of Quantum Wells (QWs) have garnered significant interest within the biomedical sector [18-21]. These properties are harnessed for a wide array of applications, including real-time tissue imaging (bioimaging) [22], diagnostics, single molecule probing, drug delivery, and more. Quantum dots offer versatility, as their optical features can be finetuned through size and composition adjustments [1]. Their remarkable attributes, such as high brightness, resistance to photobleaching, multiplexing capabilities, and a high surface-to-volume ratio, position them as ideal candidates for intracellular tracking, diagnostics, in vivo imaging, and therapeutic delivery. This study aims to explore the immense potential of colloidal materials as a viable alternative to traditional dyes in various biomedical fields. We investigate their applications and assess their suitability for a wide range of medical and biological purposes, opening new avenues for innovation and improved outcomes in these domains.

Quantum Dots and Their Properties

Nano shells represent plasmonic nanoparticles with tunable diameters ranging from approximately 10 to 300 nm. In contrast, Quantum Dots (QDs) are excitonic nanoparticles with tunable diameters of around 1 to 10 nm [23]. QDs have emerged as a novel class of fluorescent probes for molecular and cellular imaging in the realm of bioimaging. Their distinct optical and electronic properties, including size-tunable light emission, enhanced signal brightness, resistance to photobleaching, and the ability to simultaneously excite multiple fluorescence colors, surpass the capabilities of organic dyes and fluorescent proteins. These unique features

hold great promise in significantly enhancing the sensitivity of molecular imaging and quantitative cellular analysis by one to two orders of magnitude [24]. The term "dot" in quantum dots implies an extremely confined region of space, approaching zero dimensions, similar to how "wires" and "wells" in quantum terminology are confined to one and two dimensions, respectively. It is within this nanometersized realm that semiconductors undergo a transition from behaving as bulk materials to exhibiting properties predicted for individual or small groups of atoms. This transition gives rise to exceptional and unique phenomena Figure 1 [25].



In the physics of semiconductors and materials science, when a photon with energy exceeding the semiconductor's band gap energy is absorbed, it generates an electron-hole pair, commonly known as an exciton. If the semiconductor nanocrystal has a diameter smaller than its exciton Bohr radius, typically just a few nanometers, the electrons and holes become confined, giving rise to the quantum confinement effect [26]. In this state, energy levels become quantized and directly dependent on the nanocrystal's size. As the quantum dots' size decreases, typically to less than 10nm, the quantum confinement effects become more prominent. Quantum dot photoluminescence (PL) occurs when the excited electron returns to the ground state and recombines with the hole, releasing electromagnetic energy within a narrow and symmetrical energy band (frequency) [2]. This emission falls within the UV to near-infrared range. QW's are nanostructures that are typically composed of

elements from groups II-VI or III-V in the periodic table, these nanocrystals are defined by their physical size, which is smaller than the exciton Bohr radius [27,28]. For instance, in the case of spherical CdSe particles, this size threshold is around 10 nm. While extensive research over the past two decades has predominantly concentrated on the photophysics of nanostructures and their applications in microelectronics and optoelectronics [29-31], recent advancements indicate that the first practical utility of QDs is unfolding in the fields of biology and medicine [32,33]. A pivotal factor enabling these applications is the ability to synthesize large quantities of highly luminescent QDs.

Quantum Dots as Imaging Probes

In direct photoluminescence (PL) assays using quantum dots (QDs), when an excitation light source generates excitons, they can recombine and emit light energy. However, sometimes this energy can be transferred to nearby molecules without the QD emitting light. To make use of this energy transfer, a well-designed system incorporates fluorescent molecules as energy acceptors. In such a system, the transferred energy can excite an outer shell electron in the fluorescent molecule, causing it to release light (fluoresce) when the electron returns to its ground state. This energy transfer mechanism, known as Förster resonance energy transfer (FRET), was first described by Förster in 1948 [34]. Remarkably, it was not until 2001 that QD-based FRET was demonstrated in a bioassay. It is essential to note that FRET is a highly distance-dependent phenomenon, with the efficiency of energy transfer decreasing as the sixth power of the distance between the donor and acceptor.

The FRET mechanism enhances QD-based assays, allowing for the development of highly sensitive tests. FRET occurs when the donor and acceptor molecules are very close. This property enables the detection of nearby fluorophores on the QD surface. By attaching fluorophores to specific molecules, like complementary DNA sequences, QD-based FRET can identify the presence of target molecules and DNA sequences. For example, we used biotin-conjugated DNA capture probes and Cy5 fluorophore-conjugated reporter probes that hybridized with target DNA. When streptavidin-coated QDs were added, they formed complexes (QD-[capture probe]-[target DNA]-[reporter probe]). It is explained schematically in the Figures 2A-2C.

In the presence of target DNA, excited QDs emitted light and transferred energy to the reporter probes. The emitted light from both QDs and reporter probes was simultaneously detected using a custom confocal spectroscopic setup. The nanosensor assay demonstrated sensitivity over 100 times better than conventional molecular beacon DNA detection methods.



Figure 2: Nanoscale DNA Sensing with QD-Fluorophore Nanosensors: (A) Streptavidin-coated quantum dots (QDs) selectively bind to target DNA molecules that have been hybridized with pairs of complementary probes, each labeled with either a fluorophore or biotin. (B) When illuminated, both the quantum dots (QDs) and the fluorophores emit light simultaneously through photoluminescence and Förster resonance energy transfer (FRET), respectively. (C) A custom microcapillary-based detection system is employed to detect the emitted light, enabling the precise analysis of individual nanocomplexes. Adapted from the original work of the authors Zhang CY, et al. [35].

OD-Based Charge Transfer Multiplexing: **OD-based** fluorescence multiplexing is widely used in biological assays. Beyond common approaches, multiplexing signals can also be achieved by transferring charge (electrons) between ODs and nearby redox complexes. For instance, Medintz IL, et al. [36] demonstrated controlled quenching of QD photoluminescence using charge-transfer interactions between QDs and ruthenium phenanthroline (Ru-phen) complexes as illustrated in Figure 3. They connected Ruphen complexes to QDs via peptide bridges, serving as electron conduits. The transfer of charge from the metal complex to the OD surface efficiently quenched OD PL. The extent of quenching was directly related to the number of Ruphen complexes near each QD, with smaller QDs exhibiting higher quenching efficiencies due to their greater surface state density. This approach enabled multiplex quenching across a wide optical spectrum, with at least eight optical channels resolved. Applications include biosensors for proteins, maltose, fatty acids, DNA hybridization, and monitoring enzymatic activity. This interaction may find uses in multicolor fluorescence barcodes and multiplex small molecule detection, such as DNA.



Figure 3: Selective Quenching of Quantum Dot Emissions by Ru-phen Complexes via Peptide Linkage: Quantum dots (QDs) with distinct emission spectra are specifically linked to Ru-phen complexes through a peptide bridge, resulting in the precise quenching of their photoluminescence emissions via electron transfer from the complex to the QD surface. The degree of quenching in each QD's emission spectrum can be finely controlled by adjusting the number of complexes attached to the QD. This content is reprinted with permission from Medintz IL, et al. [36], ©2009 American Chemical Society.

Fluorescence intensity is determined by two factors: the extinction coefficient (ϵ) and the quantum yield (Φ). The extinction coefficient (ϵ) is linked to the amount of incident light absorbed per unit concentration of the dye and per unit length of the path traveled. Quantum dots (QDs) have an exceptionally high ε due to quantum confinement, making them absorb light very efficiently, with ε values as high as 3.5×[10][^]6 at low excitation wavelengths of 400 nm, far surpassing values for organic dyes like Alexa 594, with ϵ values as high as $1.3 \times [10]^{5}$ [37]. Quantum yield (Φ) measures the number of emitted photons compared to the number of absorbed photons and is crucial for assessing fluorophores' efficiency and signal intensity. High-quality QDs can have quantum yields as high as 85%, and their conjugation with proteins has minimal impact on yields. In contrast, organic dyes often see a significant reduction in quantum yield when bound to biomolecules. Therefore, QDs have significantly higher absorbance and comparable quantum yield, making them exceptionally bright for visualizing even a single dot. This brightness is particularly advantageous when marking antigens with low copy numbers per cell.

QDs have demonstrated significant potential in cancer detection, enabling precise and sensitive diagnostics. These nanoparticles offer several advantages over traditional methods using organic dyes and fluorescent proteins, making them valuable tools in immuno-histochemical analysis, single-molecule tracking, and in vivo imaging for cancer-related research and diagnosis. Their unique spectral properties empower the creation of multiplexed systems for simultaneous detection of multiple targets through multicolor imaging, Figure 4. Additionally, QDs can be conjugated with drug molecules or incorporated into QD-based drug delivery particles, allowing real-time drug tracking and image-guided therapy in cancer treatment [38]. Furthermore, QDs with tunable photophysical properties, particularly those emitting in the near-infrared range, have become vital for deep-tissue mono- and multiphoton in vivo imaging. This capability is especially advantageous in cancer research, where visualization of tumor tissues at greater depths is essential. Overall, ODs are emerging as a versatile and powerful tool in cancer detection, aiding in more effective research and treatment strategies.



Figure 4: Quantum Dot Applications for In Vitro and In Vivo Bioimaging, Targeted Delivery, and Drug Release. Additionally, we explore the challenges associated with quantum dot toxicity and examine the latest breakthroughs in mitigating this concern. Adopted from Bilan R, et al. [38].

Early Cancer Detection

Sentinel lymph node (SLN) diagnosis plays a crucial role in cancer surgery, especially in detecting metastatic cancer cells in SLNs. Near-infrared (NIR) QDs emitting at 850 nm have demonstrated superiority in SLN mapping, offering high sensitivity and minimal background during surgeries. Real-time intra-operative SLN mapping using NIR QDs has been reported for gastrointestinal tract cases, enabling accurate tumor border definition and reduced dissection size. QDs, especially self-illuminating QDs, have shown promise in tracking cancer cells and studying metastasis. Targeted delivery of QDs can be achieved by attaching specific molecules to their surface (Figure 5).



Figure 5: In vivo Targeting and Imaging of a Lung Metastasis Model Using QD-Based Nanotechnology: A Live Animal Imaging System. Reproduced from Chen C, et al. [39].

QDs have been used successfully in mouse models for cancer imaging, showing potential for precise diagnosis and real-time monitoring, such as in prostate cancer and glioblastoma cases. Furthermore, a standardized protocol for liver cancer imaging in animal models was developed using QD probes, aiding in the early monitoring of liver cancer metastasis. These findings represent significant advancements in preclinical studies, with potential for clinical application. In addition, a group has developed a standard protocol for in vivo imaging of liver cancer xenograft animal models. They successfully achieved animal imaging by injecting human hepatocellular carcinoma cell lines (HCCLM6) that overexpress alpha-fetoprotein (AFP) with antiAFP monoclonal antibody and OD-IgG probes. HCCLM6 has an increased potential for lung metastasis, making it a valuable tool for constructing a platform for the early monitoring of liver cancer metastasis.

Targeted Cancer Therapies

Quantum Dots (QDs) offer a versatile approach to engineer drug delivery systems for potential cancer treatment enhancement. The success of delivering QD/drug formulations to tumor cells hinges on certain principles:

Functionalized Surface: The nanoparticle's surface must incorporate targeting ligands for specific tumor cell delivery and allow simultaneous drug delivery.

Size Optimization: The nanoparticle size must be minimized for eventual body excretion.

Drug Confinement: The drug must be securely confined within the nanoparticle system to prevent harm to normal tissues. Still, it should release at tumor cells upon external triggers or local environmental cues.

Biocompatible Surface: The QDs' surface should be coated with a long-lasting biocompatible polymer to safeguard against degradation in biological environments.

Two Strategies Exist to Combine Qds and Drug Molecules into a Nanoparticle System

Direct Conjugation: Here, drug molecules link to the QD surface, which subsequently delivers drug-conjugated QDs to target locations. Drug release occurs in response to local biological conditions, like pH or enzyme presence.

Polymer Encapsulation: In this approach, the drug resides within a polymer nanoparticle along with either hydrophobic or hydrophilic QDs, depending on the polymer type. The entire QD/drug nanoparticle system is transported to the target site, and drug molecules are either released as the polymer degrades in low pH conditions or diffuse out from the polymer particle.

One study involved QD-Aptamer(Dox) conjugates, where the QD surface was tailored with an RNA aptamer recognizing prostate cancer cells [40] see Figure 6. The anticancer drug, Dox, intercalated with the RNA aptamer, was gradually released from the QD system. Another study employed nanoconjugates of CdSe/CdS/ZnS QD and doxorubicin [41], targeting alveolar macrophages for the treatment of pulmonary disease. In both cases, the released drug maintained its bioactivity. These examples illustrate the potential of nanoparticle platforms in targeted therapy and sensing applications. This makes QDs able to revolutionize drug delivery systems, enhancing their precision and efficacy, particularly in the context of cancer treatment and other medical applications.



Figure 6: (a) Schematic of QD–Apt(Dox) Bi-FRET system: QDs are surface-functionalized with A10 PSMA aptamer. Dox intercalation into the A10 PSMA aptamer on QD surface results in QD–Apt(Dox) formation and quenching of both QD and Dox fluorescence through Bi-FRET. (b) Schematic of QD–Apt(Dox) uptake into cancer cells: QD– Apt(Dox) conjugates are specifically taken up by target cancer cells through PSMA-mediated endocytosis. Dox release from QD–Apt(Dox) induces fluorescence recovery from both QD and Dox, allowing intracellular Dox delivery sensing and synchronized cancer cell localization and treatment. Adopted from Yong KT, et al. [41].



Nanocarriers are popular for precise drug delivery, enhancing drug bioavailability, targeting tumor cells, and reducing toxic effects. They can be modified through controlled chemosynthesis, carry multiple drugs, and optimize drug release. Nanocarriers interact with biomolecules, improving stability and circulation time. Various strategies involve targeting molecules and delivery vehicles. However, challenges like tumor complexity and drug metabolism persist (Figure 7).

Although significant progress has been made in targeted drug delivery in oncotherapy, many challenges and limitations, such as the complexity of tumor structure, the ambiguous biosafety of delivery systems, as well as the rapid metabolism and clearance of drugs, still remain. Therefore, further research is still necessary to promote the development and clinical application of targeted drug delivery technologies in efficient oncotherapy [43,44]. In light of the above considerations, as shown in Figure 7.

Cadmium-based ODs are widely used for in vitro and in vivo studies, despite their known toxicity due to cadmium and selenium content. Cadmium, a potential carcinogen, can distribute throughout the body, with liver and kidneys as major target organs. Recent studies have shown increasing cadmium concentration in these organs after intravenous injection of cadmium-based QDs in small animals, suggesting QD degradation in vivo. Researchers are now working on cadmium-free QDs, like InP QDs, which offer advantages such as robust covalent bonds, reduced toxicity, and ease of dispersion in aqueous systems. These cadmium-free QDs have potential for targeted delivery to tumor cells. However, comprehensive research on biocompatible cadmium-free QDs for in vitro and in vivo applications is still limited, presenting both opportunities and challenges in the QDs community [45].

Challenges and Future Prospects

Nanotoxicology, while quantum dots (QDs) show great promise in biomedical imaging and detection, concerns about their toxicological and pharmacological effects, mainly related to heavy metal content and colloidal instability. present significant hurdles to their application in cancer diagnosis and therapy [46]. These concerns may not be as problematic for in vitro applications but pose substantial barriers to their safe use in human in vivo cancer imaging. Efforts have been made to develop novel QDs with reduced toxicity and enhanced detection efficiency, considering their components, sizes, surface coatings, and valences. However, challenges like coating shell degradation due to QD modifications must be addressed. Moreover, nonspecific accumulation by the reticuloendothelial system (RES), including the liver, spleen, and lymphatic system, as well as immune responses and genotoxic effects, have been reported [46,47]. Some studies have indicated that QDs smaller than 5 nm can be excreted by the kidneys, offering potential biosafety for in vivo applications. To ensure safety, comprehensive long-term studies are required to investigate QD degradation, excretion, persistence, and immune

responses systematically. To mitigate the toxicity concerns associated with elements like Cd, Se, Zn, Te, Hg, and Pb, researchers have developed low-toxicity ODs, for instance, by substituting Cd with Zn [48]. These doped QDs exhibit reduced sensitivity to environmental factors and offer good quantum efficiency, making them promising candidates to reduce QD cytotoxicity. They also have narrow emission spectra and can cover most of the visible spectral range. In the future, doped QDs emitting in the near-infrared (NIR) region may be developed. However, extensive research and scrutiny are necessary to understand the toxicity profiles and clearance mechanisms of these QDs from living systems. **Generation of Biocompatible** Design and and Biodegradable Nanoparticles: The application of QDs in in vivo imaging and targeting is constrained by nonspecific organ uptake and RES clearance. This is primarily due to the relatively large size (15 nm to 30 nm) and short circulation half-life in the bloodstream. To address this limitation, current research focuses on extending QDs' circulation time by attaching passivating molecules like PEG and controlling particle charges to prevent plasma protein adsorption. Additionally, achieving clearance from the body is essential for clinical use. Recent findings suggest a size threshold (5 nm to 6 nm in diameter) below which QDs cannot escape the liver and are cleared through the kidneys [49].

Reproducibility, Reliability, and Comparability of QDs: The clinical application of QDs faces limitations in terms of data on reproducibility, comparability, and quantifiability. QDs with different surface functionalizations from various sources may exhibit varying fluorescence quantum yields due to differences in materials and surface chemistries. Establishing quality criteria for differently functionalized QDs is an essential first step [50-55].

Conclusions

To summarize, QDs are promising technological innovations with the potential to revolutionize cancer diagnosis and treatment. They are currently widely used in vitro for tasks like detecting cancer biomarkers, studying cancer invasion, exploring the tumor microenvironment, and improving our understanding of tumor heterogeneity, diagnosis, classification, and treatment. However, complex in vivo studies still face challenges in identifying dominant and compensatory mechanisms in tumor invasion and the microenvironment. In clinical settings, optical imaging is suitable for tissues near the skin's surface, accessible via endoscopy or intraoperative visualization. The future of nanomedicine lies in multifunctional nanoplatforms that combine therapeutic components and multimodal imaging. The ultimate goal is to develop nanoplatform-based agents that enable efficient and specific in vivo targeted drug delivery without systemic toxicity. This should also allow accurate noninvasive measurement of delivered doses

and therapeutic efficacy over time. However, challenges like inefficient delivery, potential toxicity, and a lack of quantification remain significant obstacles to the clinical translation of QDs.

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